

Target-Cell-Specific Delivery, Imaging, and Detection of Intracellular MicroRNA with a Multifunctional SnO₂ Nanoprobe**

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MicroRNAs (miRNAs) are a class of short, endogenous, noncoding regulatory RNAs (approximately 18–25 nucleotides), encoded in the genomes of plants, animals, and viruses.^[1–3] They partially complement the 3' untranslated region of target mRNAs, causing mRNA cleavage or inhibiting protein synthesis within the Dicer/Argonaute complex.^[4,5] MiRNAs play key regulatory roles in a diverse range of biological processes, including cell development,^[6] differentiation,^[7] metabolism,^[8] and apoptosis.^[9] In particular, distinct miRNA expression patterns are associated with various cancer phenotypes.^[10–12] Therefore, miRNAs are also an emerging class of useful diagnostic and prognostic markers.^[13–15] However, miRNA analysis is challenging owing to the unique characteristics of miRNAs, such as their small size, sequence similarity among family members, low abundance, susceptibility to degradation, and the technical impediments in delivering miRNAs across the plasma membrane of cells. An improved delivery strategy is thus needed to successfully monitor intracellular miRNA levels in situ.^[16,17]

Generally, transmission of oligonucleotides for gene therapy falls into two broad categories, viral vectors^[18,19] or nonviral carriers.^[20–24] Viral vectors exhibit high transfection efficiency but also some fundamental problems, such as immunogenicity and toxicity. These problems limit their broad application.^[18,19] Currently, the nonviral vectors, such as

liposomes,^[20] cationic polymers,^[21] dendrimers,^[22] polypeptides,^[23] and nanomaterials^[24] have attracted significant interest, owing to their good biocompatibility and potential for large-scale production, in contrast to viral vectors.^[25] However, many of these carrier systems do not inhibit genes in a cell-specific manner and cannot be used to monitor their intracellular delivery or therapeutic response.^[26,27] An excellent nonviral vector should efficiently facilitate cell-specific gene-probe (a single-stranded oligonucleotide designed to recognize a single target-nucleotide sequence) uptake and gene-probe endosomal escape for intracellular delivery.^[28] Fluorescent nanoparticles are highly attractive materials for gene-probe delivery because of their unique properties, including uniform size, superior imaging characteristics, and facile surface modification.^[29,30] The rational functionalization of these nanomaterials with target-specific moieties, such as antibodies,^[31] aptamers,^[32] and other molecules,^[33] to recognize receptors on the cell surface has led to versatile theragnostic nanosystems. These multifunctional nanosystems not only allow efficient delivery of gene probes to target cells with fewer side effects, but also allow the simultaneous monitoring of delivery and the therapeutic response of the targeted genes, using the advanced optical properties of the nanosystem. However, these nanosystems have not been used for in situ detection of intracellular miRNAs yet, because the detection strategy has not been optimized.

In this study we design a novel multifunctional SnO₂ nanoprobe (mf-SnO₂), which contains a cell-targeting moiety, as well as a conjugated gene probe to specifically recognize the target sequence, thus providing a detection strategy or inhibitor. Also, visualization of the delivery and intracellular response is possible through fluorescence of the SnO₂. As shown in Scheme 1, cell-specific delivery is achieved by functionalizing SnO₂ nanoparticles (SnO₂NPs) with folic acid (FA), which targets cancer cells; a gene probe, in this case a molecular beacon (MB) to detect target miRNAs, is conjugated by a disulfide linkage, which is sensitive to pH values. Cleavage of the disulfide linkage between the gene probe and the nanoparticle enhances the efficiency of intracellular delivery.^[26,34] Using miRNA-21 in HeLa cells as a model, a method for in situ detection of intracellular miRNA by the multifunctional nanoprobe is reported.

To verify the practicality of this approach, another nanoprobe was also designed, by substituting the MB with an anti-miR of miRNA-21, to down-regulate the expression of a target miRNA. The proposed method, with a MB as the recognition probe, can be used subsequently to monitor the change in miRNA levels from negligible cytotoxicity, and to monitor the ability of the multifunctional nanoprobe to

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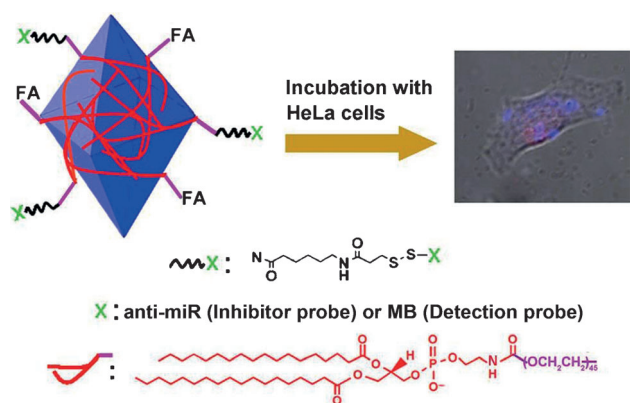
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Scheme 1. Schematic representation of mf-SnO₂ nanoprobe for target-specific-cell imaging and intracellular detection of miRNA. FA = folic acid, MB = molecular beacon.

protect gene probes from nuclease digestion or interaction with single-stranded DNA binding protein (SSB).

The structure of SnO₂NPs was confirmed by X-ray diffraction (XRD; Figure S1, Supporting Information). All of the peaks in the XRD pattern could be indexed to the rutile phase of SnO₂ (JCPDS No. 41-1445). The scanning electron microscope (SEM) image of the SnO₂NPs showed a well-proportioned octahedral structure with surface roughness. The size of the NPs was estimated to be approximately 60 nm in width and 80 nm in length (Figure 1a). The transmission electron microscope (TEM) image taken from the apex of the nanoparticle along the [110] direction further demonstrated an octahedral structure and confirmed the estimated size (Figure 1b), which was in agreement with reported values.^[35] Dynamic light scattering (DLS) measurements showed the hydrodynamic diameter of the SnO₂NPs to be about 80 nm with a narrow size distribution (Figure 1c). Also, Brunauer–Emmett–Teller adsorption–desorption isotherm curves

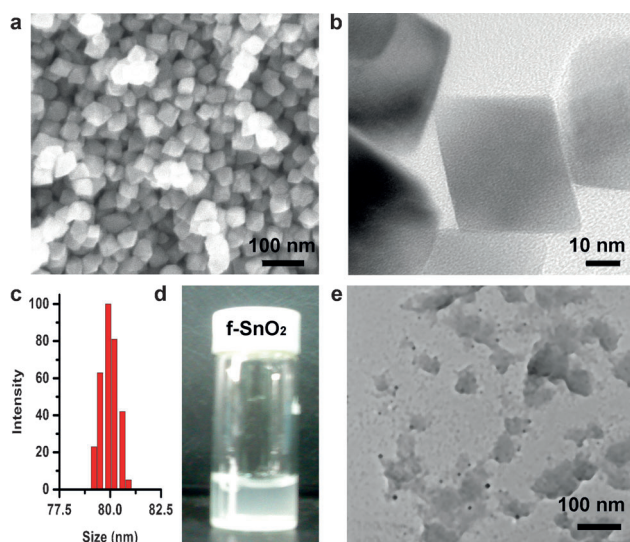


Figure 1. a) SEM, b) TEM, and c) DLS characterization of SnO₂NPs. d) f-SnO₂ functionalized with DL-PEG₂₀₀₀-FA and DL-PEG₂₀₀₀-SPDP, in PBS (pH 7.2, 0.1 M) containing serum proteins (10%). e) TEM image of f-SnO₂.

showed that the SnO₂NPs were porous, with an average pore diameter of 10.4 nm (Figure S2, Supporting Information). The SnO₂NPs emitted strong photoluminescence, with a band at 467 nm and a full-width at half maximum (FWHM) of 40 nm (Figure S3, Supporting Information).

A stable aqueous suspension of SnO₂NPs could be obtained by noncovalently functionalizing the SnO₂NPs with 1,2-distearoyl-*sn*-glycero-3-phosphoethanolamine-*N*-[amino (polyethylene glycol)₂₀₀₀] (DL-PEG₂₀₀₀) conjugated to FA (DL-PEG₂₀₀₀-FA) or sulfosuccinimidyl-6-(3'-(2-pyridyl-dithio)propionamido)hexanoate (DL-PEG₂₀₀₀-SPDP; Figure 1d). These moieties were adsorbed on the nanoparticles through van der Waals and hydrophobic interactions.^[36] The hydrophilic PEG chain extended into the aqueous phase to solubilize the DL-PEG₂₀₀₀-FA- and DL-PEG₂₀₀₀-SPDP-functionalized SnO₂NPs (f-SnO₂) in phosphate buffered saline (PBS) containing serum proteins (Figure 1e), which approximates physiological conditions. Compared to the SnO₂NPs, the TEM image of f-SnO₂ showed a smooth surface and increased size (Figure 1e). The appropriate size and good fluorescent properties combined with the stable solubility under physiological conditions, make the SnO₂NP a promising carrier for oligonucleotides. The zeta-potential analysis and electrochemical impedance spectrum analysis confirmed that SnO₂NPs were successfully functionalized with both DL-PEG₂₀₀₀-FA and DL-PEG₂₀₀₀-SPDP-MB (gene probe, Figure S4, Supporting Information).

Oligonucleotides, such as anti-miR, are susceptible to degradation by cellular nucleases during delivery into the cells.^[37–39] Therefore, an efficient delivery vector should protect the cargo against nuclease digestion and SSB interaction during prolonged transport. Herein, the ability of multifunctionalized SnO₂NPs (mf-SnO₂) to resist nuclease cleavage and SSB interaction during the recognition of the target sequence by the MB was examined. After incubating the mixture of mf-SnO₂ and miRNA-21, a sharp increase of fluorescence from the carboxyfluorescein (FAM) labeled MB was observed (Figure S5, Supporting Information), indicating specific recognition of miRNA-21 and successful conjugation of f-SnO₂ with the MB. DNase I nuclease digestion and SSB interaction experiments demonstrated that the mf-SnO₂ nanoprobe could protect the MB from nucleases (Figure S6A, Supporting Information) and interfering proteins (Figure S6B, Supporting Information). The protective effect could be from shielding by the f-SnO₂ and/or the conformational change of nucleic acid strands in the presence of f-SnO₂, both of which have been seen with carbon nanotubes.^[40,41]

The cytotoxicity of f-SnO₂ was studied using 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT) assay and an apoptosis assay. As a control, the cytotoxicity of commercial transfection agents, Lipofectamine 2000 (Lp2000) and polyethyleneimine (PEI), was also evaluated. The f-SnO₂ displayed low cytotoxicity with HeLa cells in the range from 20 mg L^{−1} to 320 mg L^{−1} (Figure 2a). The f-SnO₂-transfected cells showed 94.9% viability at the concentration of 100 mg L^{−1}, while the cells treated with PEI and Lp2000 exhibited 88.7% and 84.8% viability, respectively (Figure 2b), indicating lower cytotoxicity of the NPs, although the error in these measurements is not sufficient to

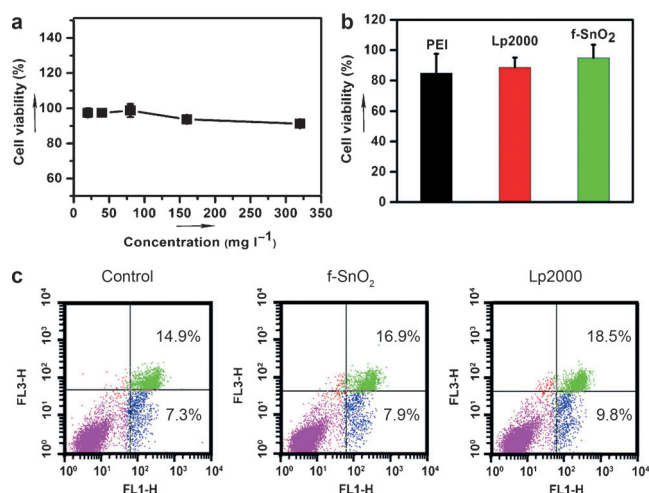


Figure 2. a) Cytotoxicity induced by f-SnO₂ at different concentrations (20, 40, 80, 160, 320 mg L⁻¹) in HeLa cells. b) Cytotoxicity induced by PEI (0.05 mM), Lp2000 (0.2 μ L per 100 μ L medium) and f-SnO₂ (100 mg L⁻¹). c) Flow-cytometric analysis of apoptosis in HeLa cells and HeLa cells transfected by f-SnO₂ (100 mg L⁻¹) or Lp2000 (0.2 μ L per 100 μ L medium). Normal cells (purple), apoptotic cells in late phase (green) and in early phase (blue); FL1-H = Annexin V positive cells, FL3-H = PI positive cells.

establish statistical significance. The lower cytotoxicity of f-SnO₂ than both PEI and Lp2000 could result from the negative surface charge, which will lower NP adhesion to the cell surface, decreasing the necrosis that is seen with positively charged PEI.^[42] The difference in cytotoxicity could also be attributed to the nontoxic composition of f-SnO₂, unlike some quantum dots containing toxic elements, such as cadmium.^[43,44] In comparison to the control group with 7.3% of cells being apoptotic, 7.9% of f-SnO₂-transfected cells were apoptotic, according to Annexin V-FITC and propidium iodide (PI)-labeling flow-cytometry analysis (Figure 2c). The f-SnO₂ displayed 20% lower apoptosis than the commercial transfection agent Lp2000. These results suggest that f-SnO₂ is a relatively safe transfection agent.

In principle, it is possible to employ the fluorescent f-SnO₂ for live-cell imaging and monitoring of the intracellular transfection efficiency (Figure S7, Supporting Information). Target-cell-specific delivery has been regarded as important for the development of therapeutics, because it can limit side effects from nonspecific delivery and reduce the quantity of gene probe needed for treatment.^[45] Herein FA, a ligand with high affinity to the folate receptor (FR), which is over-expressed on many human cancer cells causing rapid proliferation,^[46] was conjugated to the SnO₂NPs as a target-specific moiety. To confirm the specific FR-mediated transfection of the f-SnO₂, competitive binding tests with free FA and the transfection of f-SnO₂ without the presence of FA (N-f-SnO₂) were carried out. As expected, a gradual increase of fluorescence intensity, which came from the emission of the SnO₂NPs, was observed in the f-SnO₂ transfected cells, indicating the gradual uptake of the f-SnO₂ (Figure 3a, left column). In contrast, fluorescence was almost undetectable after the cells were treated with free FA for 1 hour and then transfected with the f-SnO₂ (Figure 3a, middle column). The

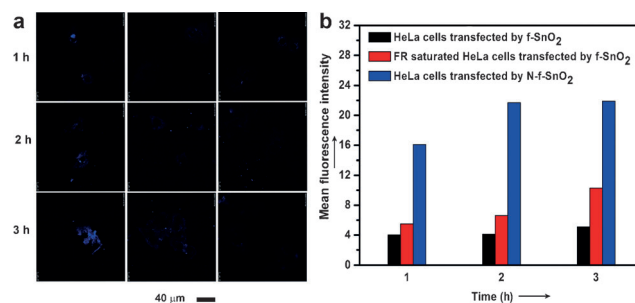


Figure 3. a) Confocal images of HeLa cells transfected with f-SnO₂ (left, 100 mg L⁻¹), FR-saturated HeLa cells transfected with f-SnO₂ (middle, 100 mg L⁻¹), and HeLa cells transfected with N-f-SnO₂ (right, 100 mg L⁻¹) at 37°C at marked times. b) Corresponding fluorescence intensities of (a). Blue field = SnO₂NP fluorescence.

lack of f-SnO₂ uptake was due to the occupancy of FRs on the cell surface by free FA molecules, which reduced the receptor-mediated endocytosis.^[47] In absence of FA, the transfection of N-f-SnO₂ also showed little uptake (Figure 3a, right column), indicating the nonspecific uptake of nanoparticles was negligible. The mean fluorescence intensities per cell are shown in Figure 3b, which highlights the differences in the uptake of f-SnO₂. FA receptor-negative A549 cells and FA receptor-positive MCF-7 cells also were treated with f-SnO₂ under similar conditions to the HeLa cells; higher fluorescence was detected in MCF-7 cells, further verifying the FR-mediated endocytosis of f-SnO₂ (Figure S8, Supporting Information). The FA-conjugated SnO₂NPs could be used as a target-cell-specific transfection reagent.

To evaluate the transfection capability of f-SnO₂ into HeLa cells, a transfection probe (TP: a FAM-labeled, single-stranded DNA of random sequence, see Supporting information) was conjugated to f-SnO₂ using a disulfide linkage. After the resulting mf-SnO₂-TP (also conjugated with FA) was internalized into cells by FR-mediated endocytosis, the disulfide linkage between TP and f-SnO₂ can be cleaved in the reductive and acidic intracellular environment^[47–49] to release the TP (Figure S9, Supporting Information), which enhanced the efficiency of intracellular delivery.^[50] The internalization could be confirmed by the TEM images, while the confocal microscopic images indicated some cleavage of the mf-SnO₂-TP (Figure S10, Supporting Information). The transfection efficiency of mf-SnO₂-TP (100 mg L⁻¹, 50 nM linked TP) was assessed in comparison to a commercial transfection agent Lp2000-TP (0.2 μ L per 100 μ L medium, 50 nM TP) and a typical polymeric vector^[21] PEI-TP (0.05 mM, 50 nM TP). The results indicated the promising transfection efficiency of the mf-SnO₂-TP (Figure S11, Supporting Information).

MiRNA mutation or dysregulation is associated with various human cancers.^[51,52] Thus, methods to detect or inhibit intracellular miRNAs are useful in finding new biomarkers for clinical diagnosis and new targets for gene therapy. Using miRNA-21, linked to several cancers,^[53,54] as a model, the inhibitor probe anti-miR of miRNA-21 was conjugated to f-SnO₂ by disulfide bond, to down-regulate the level of the miRNA-21. The intracellular miRNA-21 level was monitored

by confocal microscopy after target-cell-specific delivery of mf-SnO₂-MB into the cells. After the cells were incubated with the FA-conjugated mf-SnO₂-anti-miR for 48 h to inhibit the miRNA expression, the fluorescence intensity of FAM-labeled MB was 40.9% of that without miRNA-21 down-regulation (Figure 4, red field). This result was verified by reverse-transcriptase quantitative PCR (RT-PCR) analysis, which showed 49.4% down-regulation (Figure S12, Supporting Information). Thus, the designed multifunctional SnO₂ nanoparticle could be used for both regulation and in situ monitoring of intracellular miRNA levels.

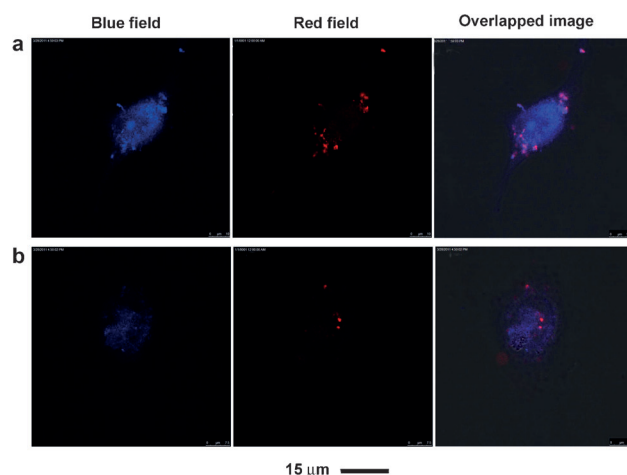


Figure 4. a) Confocal images of HeLa cells transfected with mf-SnO₂-MB (100 mg L⁻¹, 50 nm linked MB) at 37°C for 3 h. b) HeLa cells first transfected by mf-SnO₂-anti-miR (100 mg L⁻¹, 50 nm linked anti-miR) at 37°C for 3 h and detected with mf-SnO₂-MB (100 mg L⁻¹, 50 nm linked MB) 48 h later. Red field = FAM-labeled MB, blue field = SnO₂NP fluorescence.

To assess detection of intracellular miRNA, different amounts of miRNA-21 mimics (Sequences found in the Supporting information; <http://microrna.sanger.ac.uk/sequences>) were transfected into the cells, which were then transfected with mf-SnO₂-MB to obtain a calibration curve. The red fluorescence intensity, measured by confocal microscopy, increased with increasing amount of miRNA-21 mimics in the cells, (Figure 5a). The plot of fluorescence intensity versus the amount of miRNA-21 mimics transfected into a single cell, up to 11.3 pg, showed a linear relationship, with a related coefficient of 0.995 (Figure 5b). From the linear regression equation and the fluorescence intensity of FAM from the HeLa cells, the average quantity of miRNA-21 in a single HeLa cell can be calculated as 1.63 pg. All of these experiments describe an effective imaging method for in situ detection of intracellular miRNA.

In summary, this work develops a multifunctional SnO₂ nanoprobe for simultaneous specific delivery, cell imaging and intracellular miRNA detection. The mf-SnO₂ nanoparticle can protect conjugated oligonucleotides from nuclease digestion and SSB interaction during in vitro cellular delivery. MTT and apoptosis assays indicate the low cytotoxicity of the f-SnO₂. The FR-mediated endocytosis and cell-specific tar-

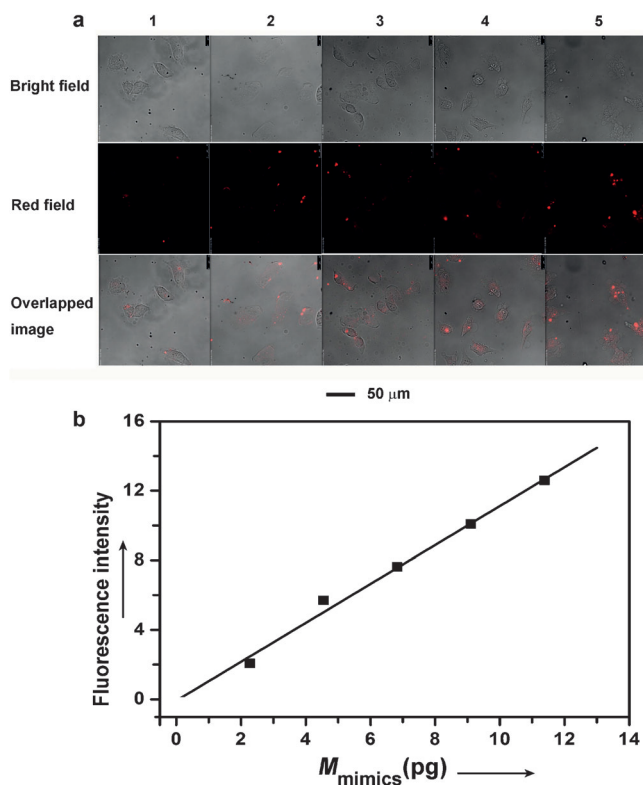


Figure 5. a) Confocal images of HeLa cells transfected with Lp2000-miRNA-21-mimics (0.2 μL per 100 μL medium) mixed with different amounts of miRNA-21 mimics (the quantity internalized by a single HeLa cell was 2.27, 4.55, 6.83, 9.11 and 11.38 pg from 1 to 5, respectively) at 37°C for 3 h, then detected with mf-SnO₂-MB (100 mg L⁻¹, 50 nm linked MB). b) Plot of fluorescence intensity versus quantity of intracellular miRNA-21 mimics.

geting of f-SnO₂ by FA conjugation has been verified. An appropriate size, good fluorescent properties, solubility under physiological conditions, and high transfection efficiency make f-SnO₂ a promising target-cell-specific transfection agent. The f-SnO₂ has been further functionalized with different oligonucleotides, including a transfection probe, an inhibition probe, and a detection probe, which suggests future applications in regulating the expression of intracellular miRNA levels and in situ monitoring of the change in miRNA levels. A novel method for in situ detection of miRNAs in a single cell has also been proposed. Both the multifunctional SnO₂ nanoprobe and the methods used in this report can be applied in biomedical and clinical research.

Experimental Section

The HeLa cell line was obtained from the Jiangsu Institute of Cancer Prevention and Cure, Nanjing, China. A549 and MCF-7 cell lines were kindly provided by School of Life Science, Nanjing University. All the three cell lines were cultured in Dulbecco's modified Eagle's medium (DMEM, GIBCO) supplemented with 10% fetal calf serum, penicillin (100 mg mL⁻¹), and streptomycin (100 mg mL⁻¹) at 37°C in a humidified atmosphere containing 5% CO₂. Cell numbers were obtained using a Petroff-Hausser cell counter (USA). Serum-free medium (Opti-MEM) was used during the transfection process.

The HeLa cells (1.0×10^4) were cultured for 12 h in a 96-well plate containing DMEM (100 μ L) in each well, the medium was replaced with fresh Opti-MEM alone or medium containing f-SnO₂ (100 mg L⁻¹), Lp2000 (0.2 μ L per 100 μ L medium), or PEI (0.05 mM) to incubate for another 3 h. MTT (100 μ L, 1 mg mL⁻¹) was then added to each well. The media were removed 4 h later, and sodium dodecylsulfate (150 μ L, 0.52 M) was added to solubilize the formazan dye. After 15 min, the absorbance of each well was measured using Hitachi/Roche System Cobas 6000 (Tokyo, Japan) at 490 nm. The relative cell viability (%) was calculated by $(A_{\text{test}}/A_{\text{control}}) \times 100$.

The apoptosis experiments were carried out with Annexin V-FITC/PI double staining. The cells (1.6×10^5) were seeded for 12 h in a 6-well plate containing DMEM (2 mL) in each well. The culture medium was then replaced with Opti-MEM (2 mL) containing f-SnO₂ (100 mg L⁻¹), Lp2000 (0.2 μ L per 100 μ L medium), or PEI (0.05 mM) and cultured for another 3 h. After discarding the medium, fresh DMEM was added, and cells incubated for another 24 h. The resulting cells were harvested, and stained with Annexin V-FITC/PI for 10 min, according to manufacturer's instruction. The HeLa cells were then collected and analyzed by flow cytometry on FACS Calibur flow cytometer (Becton Dickinson, USA).

The target-cell-specific transfection was performed as follows: after HeLa cells were cultivated for 12 h in 24-well culture plates containing DMEM (500 μ L), with an initial 4×10^4 cells/well, the medium was replaced with fresh Opti-MEM (500 μ L) containing f-SnO₂ (100 mg L⁻¹) or N-f-SnO₂ (100 mg L⁻¹) at room temperature for 3 h. For the competitive test, prior to transfection with f-SnO₂ (100 mg L⁻¹), the cells were first incubated with Opti-MEM (500 μ L) containing FA (1 mM) for 1 h, to saturate the FR sites on the cell surface. The transfection of MCF-7 and A549 cells with f-SnO₂ was carried out using the same procedure.

For analysis of intracellular miRNAs with mf-SnO₂-MB, HeLa cells were cultivated on glass cover slides for 12 h, at an initial density of 4×10^4 cells/slide, which were transferred into 24-well culture plates containing DMEM (500 μ L) in each well. The medium was then replaced with fresh Opti-MEM (500 μ L) containing mf-SnO₂ (100 mg L⁻¹, 50 nm linked MB) and cultivated for 3 h. Prior to performing the confocal imaging, the cover slides were washed thoroughly and fixed on glass slides. In the inhibitor experiment, HeLa cells were first transfected with mf-SnO₂-anti-miR (100 mg L⁻¹, 50 nm linked inhibitor probe anti-miR) at 37 °C for 3 h and then 48 h later transfected with mf-SnO₂-MB (100 mg L⁻¹, 50 nm linked MB), for detection. To detect the amount of intracellular miRNA in situ, the cells were first incubated with Opti-MEM (500 μ L) containing Lp2000-miRNA-21-mimics (0.2 μ L per 100 μ L medium) and different amounts of miRNA-21 mimics and 48 h later detected with mf-SnO₂-MB (100 mg L⁻¹, 50 nm linked MB). The quantity of miRNA mimics internalized by a single HeLa cell was calculated by $(M_{\text{before}} - M_{\text{after}})/A_{\text{cell}}$ number, where M_{before} and M_{after} was the mass of mimics in the media before and after transfection calculated by the absorbance at 260 nm, respectively, and A_{cell} number was the number of transfected cells.

The details about preparation, functionalization, and characterization of SnO₂NPs, assembly and characterization of mf-SnO₂, response of mf-SnO₂-MB to target in vitro, protection properties of f-SnO₂, in vivo transfection by f-SnO₂, FA-mediated endocytosis of f-SnO₂, gel electrophoresis experiments, in vivo transfection by mf-SnO₂-TP, transfection efficiency, and reverse-transcriptase quantitative PCR (RT-qPCR) experiments are described in the Supporting Information.

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